

U.S. PATENT APPLICATION

Inventors: Laurence W. HEDLUND
Arja C.S. BRAU
Charles T. WHEELER
G. Allan JOHNSON

Invention: MR-COMPATIBLE METHODS AND SYSTEMS FOR CARDIAC
MONITORING AND GATING

*NIXON & VANDERHYE P.C.
ATTORNEYS AT LAW
1100 NORTH GLEBE ROAD
8TH FLOOR
ARLINGTON, VIRGINIA 22201-4714
(703) 816-4000
Telecopier (703) 816-4100*

SPECIFICATION

**MR-COMPATIBLE METHODS AND SYSTEMS FOR CARDIAC
MONITORING AND GATING**

GOVERNMENT RIGHTS STATEMENT

5 This invention was made with Government support under Grant
No. NIH NCRR #P41 RR05959 awarded by the National Institutes of
Health. The Government has certain rights to the invention.

FIELD OF THE INVENTION

10 The present invention relates generally to the field of magnetic
resonance (MR) imaging. More specifically, the present invention relates
to systems and methods for reliably monitoring and gating cardiac activity
in patients during MR microscopy.

BACKGROUND AND SUMMARY OF THE INVENTION

15 A fundamental problem associated with using a conventional
electrocardiograph (ECG) to monitor a patient's cardiac activity during MR
imaging is the corruption of the ECG signal due to adverse
electromagnetic effects. This effect is particularly pronounced in MR
microscopy of small animals (e.g., laboratory rodents), where strong,
rapidly-switching, magnetic field gradients are needed to obtain high
spatial and temporal resolution, and the animal's ECG signal is less than
20 a millivolt in amplitude. The spurious signals often resemble the QRS
spike and can lead to erroneous cardiac gating. Furthermore, the
artifacts often do not disappear until tens of milliseconds after the
gradients turn off.

Several methods have been proposed to improve the quality of the ECG, and alternative measures of cardiac activity have been suggested. See, Felblinger et al, *Magn. Res. Med.*, 32, 523-529 (1994); Lindberg et al, *Med. Bio. Eng. Comp.*, 30, 533-537 (1992); and Legendre et al, *Magn. Res. Med.*, 3, 953-957 (1986), the entire contents of each being incorporated hereinto expressly by reference. However, none of these conventional methods has been shown to provide reliable monitoring and gating ability in small rodents during cardiac MR microscopy. It is therefore towards fulfilling such a need that the present invention is directed.

Broadly, the present invention is embodied in noninvasive, MR-compatible methods and systems whereby mechanical cardiac activity is detected optically by movements in the esophagus and/or other anatomic structures affected by cardiac activity, such as, for example, the chest wall or blood vessels. More specifically, according to a particularly preferred embodiment of the present invention, esophageal compressions are used as a proxy for rhythmic cardiac activities. These esophageal compressions may be detected to provide a signal indicative of periods of cardiac activity and inactivity. The signal may be further processed so as to generate a trigger signal that may be input to a MR scanner. In such a manner, MR microscopy may be accomplished in such a manner so as to record images at desired specific phases of the cardiac cycle, for example to record images in synchrony with periods of cardiac inactivity. Moreover, since mechanical cardiac activity is detected and employed (i.e., by detecting physical movements in the esophagus and/or other anatomic structures affected by cardiac activity), instead of electrical activity as is employed in conventional techniques, the present invention is immune to electromagnetic interference during MR microscopy. As a

result, robust cardiac signals may be monitored and gated during 2-dimensional and 3-dimensional *in vivo* microscopy. The present invention is therefore especially well suited for MR microscopy of small animals, such as laboratory mice and rats.

5 These aspects, as well as others, will become more clear after careful consideration is given to the following detailed description of the preferred exemplary embodiments.

BRIEF DESCRIPTION OF THE ACCOMPANYING DRAWINGS

10 The patent or application file contains at least one drawing executed in color. Copies of this patent or patent application publication with color drawing(s) will be provided by the Office upon request and payment of the necessary fee.

 The present invention will be described with reference to the following drawings, wherein:

15 FIGURE 1 is a schematic view of a presently preferred system in accordance with the present invention;

 FIGURE 2 is a trace of waveforms for the detected optical signal, corresponding gating pulses, ECG and airway pressure obtained from the procedures of the Example below; and

20 FIGURES 3a and 3b are respective color screen saves of a physiologic monitor taken during fiber optic-gated, CINE cardiac MR microscopy obtained from the procedures of the Example below with the imaging gradients turned on and off, respectively.

DETAILED DESCRIPTION OF THE INVENTION

Accompanying FIGURE 1 depicts a presently preferred system 10 in accordance with the present invention, which is depicted, in an exemplary fashion, for use with a small laboratory animal, such as a mouse 12. As is well known to those in this art, the mouse 12 may be positioned within a magnet 14 associated with a magnetic resonance (MR) scanner.

The mouse 12 is intubated to insure a patent airway. An optical probe assembly 16 is inserted into the mouse's esophagus. The probe assembly 16 is most preferably comprised of at least transmit and receive optical fibers 16a, 16b, respectively. The distal end of the probe assembly 16 is positioned so as to be at a site physically within the mouse's esophagus adjacent the heart (schematically depicted in FIGURE 1 and identified therein by reference numeral 12a).

A laser diode 18 supplies laser light to the transmit optical fiber 16a so as to illuminate the site of the mouse's esophagus adjacent the distalmost end of the optical probe assembly 16. Light reflected from that esophagus site is then received by the optical fiber 16b and directed to an amplified photodetector 20 optically coupled thereto. The photodetector derives an output signal 22 from the reflected light, which is indicative of cardiac heart beats (that is, the rhythmic periods of cardiac activity and inactivity). The output signal 22 is further processed by signal processor 24 so as to supply a trigger signal 26 to a scan trigger 28 operatively coupled to the computer system associated with the MR scanner. The trigger signal 26 thus causes the scan trigger to initiate a MR scan pulse when the output signal 22 indicates a period of cardiac inactivity. Alternatively, the trigger signal 26 can be stored with the acquired MR

data for use in post-processing methods to yield a series of dynamic images demonstrating the heart at varied phases of the cardiac cycle. The signal processor 24 may also supply a monitoring signal 30 to a physiologic monitor 32.

5 The present invention will be further described with reference to the following non-limiting Example.

EXAMPLE

10 A system 10 as shown in FIGURE 1 was employed. Specifically, two 5-m step-index multimode optical fibers (Thorlabs, Newton, NJ) were used as the transmit and receive optical fibers 16a, 16b, respectively. The last 10 cm of each fiber was stripped of buffer, and the bare fibers were bundled together for total diameter of 250 microns. The fiber tips were cleaved at appropriate angles to maximize light detection. Light from a collimated 40 mW, 650 nm laser diode (Thorlabs), selected for its
15 minimal tissue absorption, was focused into the transmit fiber 16a using an optical lens.

20 Twenty-eight rats (150g-250g) and one C57 mouse (40g) were intubated and anesthetized with isoflurane delivered by a computer-controlled ventilator as described more fully in Hedlund et al, *Magn. Res. Img.*, 18, 753-759 (2000), the entire content of which is expressly incorporated hereinto by reference. Pediatric electrodes were taped to the animal's footpads to acquire a reference ECG signal. Average heart rates were 300 bpm for the rat and 400 bpm for the mouse. The bundled fiber optic probe 16 was easily inserted down the animal's esophagus to
25 the mid-chest level with the aid of a tapered catheter oriented towards the heart.

As light from the transmit fiber impinged upon the esophageal wall, the amount of reflected and scattered light detected by the second fiber 16b varied over the cardiac cycle as a result of systolic contraction. The optical signal was conveyed to an amplified photodetector 20 (Thorlabs), and the electrical signal was passed to a signal processor 24, which generated a 5 ms trigger pulse on the falling-edge of the detected signal for cardiac gating. The circuit also included an adjustable lockout period to reject arrhythmias or other spurious pulses. The optical signals were displayed on a physiologic monitor along with ECG and airway pressure waveforms. All imaging was preformed on a 2.0 T magnet (Oxford Instruments, Oxford, UK) with a 7-cm diameter radio frequency (RF) coil.

Accompanying FIGURE 2 shows, from top to bottom, the waveforms for the detected optical signal (W1), the corresponding gating pulses (W2), the ECG (W3) and the airway pressure (W4) in a rat. The periodic variations in the detected optical signal arise from reflection of the laser from the esophageal wall and the heart. The variations are greatest during inspiration, when the lungs occupy the largest volume and further compress the esophagus. The cardiac gating pulses clearly match the frequency of the ECG, joining up perfectly with the QRS spike.

Screen saves of the physiologic monitor taken during fiber optic-gated, CINE cardiac MR microscopy are shown in accompanying FIGURES 3a and 3b, and demonstrate the utility of the system in accordance with the present invention as compared to conventional ECG. In this regard, the traces shown in FIGURE 3a were obtained with the imaging gradients off and the gating pulses are coincident with the QRS spike of the ECG. In contrast, however, in FIGURE 3b, imaging gradients were turned on and the ECG trace is visibly corrupted by induced voltages, while the fiber optically derived signals from the system of the

present invention is unaffected and continues to provide a reliable cardiac signal.

5 While the invention has been described in connection with what is presently considered to be the most practical and preferred embodiment, it is to be understood that the invention is not to be limited to the disclosed embodiment, but on the contrary, is intended to cover various modifications and equivalent arrangements included within the spirit and scope of the appended claims.

10
15
20
25
30
35
40
45
50
55
60
65
70
75
80
85
90
95
100